POLYMER-CONTROLLED EXTENDED COMBINATION RELEASE OF SILVER AND CHLORHEXIDINE FROM A BONE VOID FILLER

Jason DeGooyer¹, Sherry N. Davidoff², Benjamin D. Brooks¹, David W. Grainger^{1,2}, Amanda E. Brooks²

¹Department of Bioengineering ²Department of Pharmaceutics and Pharmaceutical Chemistry University of Utah, Salt Lake City, UT 84112 USA

ABSTRACT

Although rates of total joint prosthetic infections remain relatively constant at 1-3%, an increasing number of orthopedic procedures and a corresponding rise in the absolute number of infectious complications mandate distinctly new solutions. In order to combat the implant infection threat, an antibiotic-releasing bone void filler (BVF), commercial tradename, ElutiBoneTM, has been developed using a combination of commercially available ceramic-based BVF plus clinically familiar biocompatible polymers, and a variety of select, dispersed antibiotics. While several traditional antibiotics have been successfully released for an extended duration, a more versatile strategy, releasing multiple antibiotics simultaneously, may be possible. In this study, the antiseptic chlorhexidine and a variety of bacteriostatic silver compounds were incorporated to provide synergistic antimicrobial activity upon release in combination formulations from ElutiBone matrices. Silver chloride was the most effective bacteriostatic tested ($p \le 0.05$), showing a measurable zone of inhibition at spiked concentrations as low as $31\mu g/ml$. Subsequently, silver chloride was used in combination with the antiseptic chlorhexidine to test for enhanced antimicrobial bioactivity against *S. aureus*. Measurable synergy between the two compounds confirmed the suitability of ElutiBoneTM to locally deliver this multidrug antimicrobial cocktail. A myriad of other drug interactions could and should be tested in this novel system in order to expand the utility and combat the increasing prevalence of polymicrobial infections.

Keywords: controlled release, antibiotic delivery, orthopedic infection, antibiotic combination therapy, antimicrobial allograft, polycaprolactone, osteomyelitis, combination device

INTRODUCTION

Nearly 1.3 million people in the United States received a joint prosthesis in 2010, representing a steady increase in total joint replacement (TJR) procedures over the past decade. This increased demand in conjunction with finite infection rates (1-3%) [1], and better microbial detection methods have culminated in higher absolute numbers of patients suffering with acute or chronic implant infections [2]–[5]. Furthermore, approximately 10% of primary TJRs require a revision surgery wherein recurrent infections are reported at rates 20-30%, with secondary infections running nearly 18% [6]–[8]. Three recognized primary causes for these recurrent infections are: 1) lack of device stability [9]; 2) bone's limited vascular supply, and 3) sequestra — localized areas of ischemia and necrosis that present a favorable, inert environment for harboring bacteria and allowing their unmitigated persistence in the dysvascular wound space [10], [11]. Moreover, the economic burden for surgically addressing periprosthetic infections [12]. Current clinical tools to address acute and chronic bone infection are invasive, costly, and frequently ineffective, further compromising the patient's overall health and recovery [12], [13].

Clinical approaches for treatment or prevention of PI fall into two groups, often administered simultaneously. Systemic antibiotic prophylaxis is considered the standard of care; however, studies are lacking to support this approach to PI treatment [12], [14]. While considered generally effective,

problems with systemic antibiotic delivery include systemic side effects and low antibiotic concentration at bone infection sites — potentially promoting antibiotic resistance [12], [15]. The second treatment option involves localized delivery of antibiotics directly to the site of infection. This strategy is commonly embodied by 1) surgical debridement with an antibiotic solution [16], 2) application of antibiotic solutions to bone grafts by soaking in high concentration antibiotic solutions, and 3) implantation of antibiotic-loaded bone cements. Even though surgical debridement with antibiotic solutions and physisorption of antibiotic to bone graft may provide immediate protection at the surgical site, neither alternative offers lasting efficacy. Importantly, all knee revisions, infected or not, require new bone stock, commonly supplied by bone graft (estimated 30-50 cm³ per knee) [17]–[19]. However, no current clinical technology endows this substrate with a legitimate, controlled release design for extended bioactive drug release [10], [20]-[25]. Alternatively, effort has been made to incorporate controlled local antibiotic delivery through the routine use of antibiotic-loaded bone cement (ALBC). Unfortunately, ALBC is a classic example of inadequate local antibiotic delivery controlled by a glassy, non-swelling, non-biodegradable polymer foreign body. Early burst of antibiotic is followed by extended release of drug below the therapeutic level [26]. Consequently, a new local controlled extended antibiotic delivery to treat PI is needed. The development of polymer-controlled, antibiotic bone void filler (ElutiBoneTM) is not only dependent on the substrate and the polymer matrix but also on the choice of antibiotic[23], [27].

Certain antibiotics, such as the aminoglycosides (e.g., gentamicin, tobramycin, etc.), are very amenable to incorporation in a polymer-controlled antibiotic bone void filler, such as ElutiBoneTM, due to their stability and broad spectrum activity [28]–[30]. However, the alarming rise in multidrug

resistant bacteria has somewhat neutralized the bactericidal potency of the aminoglycosides [31], thereby necessitating the investigation of new microbial compounds and cocktails. Silver has a long history of particularly use, in combination with the antiseptic [32], chlorhexidine, and may prove appropriate for local PI treatment [33]. Based on the theoretical bactericidal mechanism of action, several silver salts were incorporated in ElutiBone[™] BVF both with and without the addition of

Cohort Name	PCL (mg)	PEG (mg)	ProOsteon 500R (mg)	Silver Salts (mg)			Chlorhexidine
				AgCl	AgNO3	Ag2CO3	(mg)
Cohort 1	150	0	350	55			
Cohort 2	135	15	350	55			
Cohort 3	112.5	37.5	350	55			
Cohort 4	150	0	350		55		
Cohort 5	135	15	350		55		
Cohort 6	112.5	37.5	350		55		
Cohort 7	150	0	350			55	
Cohort 8	135	15	350			55	
Cohort 9	112.5	37.5	350			55	
Cohort 10	150	0	350				55
Cohort 11	135	15	350				55
Cohort 12	112.5	37.5	350				55
Cohort 13	150	0	350	27.5			27.5
Cohort 14	135	15	350	27.5			27.5
Cohort 15	112.5	37.5	350	27.5			27.5

Table 1. Compositional comparison of all drug-loaded BVF sample cohorts used in

chlorhexidine to assess both the potency and synergy of drug release from this combination device in the course of this study (Table 1). Synergy is defined as an increase in the duration or efficacy of antimicrobial bioactivity when compared to either drug individually. By using a combination release strategy, ElutiBoneTM has proven an effective platform for tailored, extended-duration antimicrobial release to address the complex clinical needs associated with periprosthetic orthopedic infections.

METHODS

Fabrication: ElutiBone composite BVF was fabricated as previously described[23][31]. Briefly, ProOsteon 500R (Biomet, USA) was morselized and sieved to select for particulate between 150-425µm. Polycaprolactone 10 kD (PCL, Sigma, USA) was mixed with polyethylene glycol (PEG, Sigma, USA) and then heated at 75°C to produce a molten polymer blend. The morselized ceramic, ProOsteon, and antibiotics (See table 1) were added as solids and mixed into polymer blend to form a composite matrix (n=3). The molten composite matrix was then compressed into a silicone mold (2 mm x 3 mm x 6 mm) and cooled to room temperature, forming a composite solid.

Drug Concentration Standards: Concentration standards were made in PBS for each of three silver salts (Sigma) and chlorhexidine (Sigma) from zero to 8 mg/ml (n=2). Each standard (500 µl) was used in subsequent bioactivity assays.

Antibiotic Bioactivity: Known masses of ElutiBone drug-loaded combination devices were incubated in PBS at 37°C. PBS was completely exchanged at 24h, 72h, and each week out to 12 weeks. The bioactivity of antibiotic released into the PBS milieu was determined via zone of inhibition assays (ZOIs). ZOIs were determined on BHI (Brain Heart Infusion) agar plates using 10⁵ CFU of *S. aureus* according to standardized CLSI methods [35] and as previously described. *Staphylococcus aureus* (ATCC strain 49230) was cultured as previously described [23][34].

RESULTS

In this study, the antiseptic chlorhexidine and a variety of bacteriostatic silver compounds were incorporated into ElutiBoneTM BVF combination devices to investigate potential synergistic



antimicrobial activity against S. aureus, the most commonly causative organism in PI. Each agent - silver chloride, silver nitrate, and silver carbonate - was released from ElutiBone[™], and their antimicrobial efficacy assessed. Silver salts are ionized to inhibit bacterial growth through interaction with cellular membrane channels, receptors and enzymes, and subsequent damage to membranes and intracellular metabolic activity [36]. No bioactivity was seen from silver carbonate release, potentially due to limited solubility. Based intrinsic on initial concentration standards, silver chloride was found to be the most effective silver salt for inhibiting growth of S. aureus bacterial cultures in vitro ($p \le 0.05$) (see Figure 1).

Chlorhexidine was also released from ElutiBone[™] to determine its efficacy. As a cationic bisbiguanide, chlorhexidine interacts with the cellular membrane followed by leakage of the intracellular contents[37]. Alone, chlorhexidine shows consistent inhibition for only three days (Figure 2A), indicating a rapid burst of drug from the combination BVF device.

Silver chloride was subsequently the only silver salt pursued in combination with the antiseptic chlorhexidine to assess synergistic or enhanced dual antimicrobial bioactivity against *S. aureus* beyond that seen with either individual compound. Results revealed that over the 12-week *in vitro* study, 69% of the antimicrobial assays displayed a significantly larger zone of inhibition when compared to either drug alone and seemed to be synergistic in their antimicrobial activities ($p \le 0.05$, Figure 2), irrespective of the BVF polymer ratio, confirming the concept that ElutiBoneTM BVF can be formulated to release multidrug cocktails to produce longer-term more powerful antimicrobial effects than each drug alone. Importantly, the duration of antimicrobial efficacy was also increased with higher amounts of PCL in the polymer matrix.



DISCUSSION

Implantable local antibiotic delivery devices at orthopedic surgical sites remain among the most promising tools in infection rate reduction [27][32]. Local delivery of antibiotic mitigates resident pathogens, reduces problems of systemic toxicity, and maintains drug concentrations above the MIC at the surgical site. These properties also reduce the potential for development of antibiotic resistance [23][32][34]. Unfortunately, current standard of care for localized orthopedic drug delivery relies primarily on non-degrading, antibiotic-releasing, poly(methylmethacrylate) glassy matrices [26][38] that fail to meet the relevant regulatory and clinical criteria for use as a local antibiotic-eluting device and that create permanent foreign body implants. Thus, the problem of orthopedic infection will remain until a better and more complete solution (i.e., implant/surgery/antimicrobial protocol) is implemented.

In previous studies, we have detailed how ElutiBone[™] BVF addresses many of these orthopedic infection problems [23][32][34]. To date, most of this work uses BVF designs incorporating tobramycin. Thus the scope of this study has served to further broaden the possibilities of drugs that may be used in ElutiBone[™] BVF technology. Combinations of silver chloride/chlorhexidine provide an intriguing released cocktail due to the observed synergy (i.e. enhanced antimicrobial bioactivity) and extended release profile. As a single compound release, chlorhexidine was only able to provide reliable inhibition

for 3 days (Figure 2a). Chlorhexidine is known to inhibit the growth of susceptible staphylococci at an MIC <4mg/L [39], as indirectly confirmed in Figure 1 where all standards inhibited bacterial growth. Importantly, silver chloride was determined to be the most effective silver salt, potentially due to the compound's favorable solubility and ready ionic release. The silver/chlorhexidine combination, already commercialized for antimicrobial catheter use, potentially provides additional benefit, reducing the potential for development of antimicrobial resistance [32]. Reducing the propensity for the development of multidrug resistance is critical in this system as periodic, transient pauses in bioactivity are observed (Figure 2C); however, this is not thought to be an overwhelming obstacle due to the high level of inhibition seen through 6 weeks and the intermittent strong inhibition of microbial growth to 12 weeks. Nevertheless, a thorough investigation of the release kinetics of this BVF combination device must be more thoroughly evaluated for extended durations of sub-MIC drug release.

Many other drug interactions could and should be tested in this novel system in order to broaden the scope of BVF antimicrobial efficacy. Future work will focus on *in vivo* performance and antiinfective efficacy for this combination medical device in preclinical infection models as well as detailing the mechanism of killing and extended agent release from this degradable antimicrobial BVF.

ACKNOWLEDGMENTS

Biomet is thanked for generously providing ProOsteon 500R biomedical grade coralline hydroxyapatite granules. ElutiBoneTM is a protected trademark of Elute, Inc. (Salt Lake City, USA) and used with permission. This work was supported both by the University of Utah Technology Commercialization Office, the University of Utah's Office of Undergraduate Education and Elute, Inc. (Salt Lake City, USA). Authors AEB and DWG have a financial interest in Elute, Inc., Salt Lake City, USA. Authors BDB, DWG, and AEB hold the patent on the drug release technology described herein and licensed from the University of Utah.

REFERENCES

- [1] C. Ketonis, S. Barr, C. S. Adams, N. J. Hickok, and J. Parvizi, "Bacterial colonization of bone allografts: establishment and effects of antibiotics," *Clin. Orthop.*, vol. 468, no. 8, pp. 2113–2121, Aug. 2010.
- [2] D. Campoccia, L. Montanaro, P. Speziale, and C. R. Arciola, "Antibiotic-loaded biomaterials and the risks for the spread of antibiotic resistance following their prophylactic and therapeutic clinical use," *Biomaterials*, vol. 31, no. 25, pp. 6363–6377, 2010.
- [3] E. M. Hetrick and M. H. Schoenfisch, "Reducing implant-related infections: active release strategies," *Chem. Soc. Rev.*, vol. 35, no. 9, pp. 780–789, 2006.
- [4] A. Trampuz and A. F. Widmer, "Infections associated with orthopedic implants," *Curr. Opin. Infect. Dis.*, vol. 19, no. 4, pp. 349–356, Aug. 2006.
- [5] W. Z. M.d and A. Trampuz, "Biomaterial-Associated Infection: A Perspective from the Clinic," in *Biomaterials Associated Infection*, T. F. Moriarty, S. A. J. Zaat, and H. J. Busscher, Eds. Springer New York, 2013, pp. 3–24.
- [6] L. O. Conterno and C. R. da Silva Filho, "Antibiotics for treating chronic osteomyelitis in adults," *Cochrane Database Syst Rev*, vol. 3, 2009.
- [7] C. B. Landersdorfer, J. B. Bulitta, M. Kinzig, U. Holzgrabe, and F. Sörgel, "Penetration of antibacterials into bone," *Clin. Pharmacokinet.*, vol. 48, no. 2, pp. 89–124, 2009.
- [8] S. Kurtz, F. Mowat, K. Ong, N. Chan, E. Lau, and M. Halpern, "Prevalence of primary and revision total hip and knee arthroplasty in the United States from 1990 through 2002," *J. Bone Jt. Surg.*, vol. 87, no. 7, pp. 1487–1497, 2005.
- [9] W. C. Schroer, K. R. Berend, A. V. Lombardi, C. L. Barnes, M. P. Bolognesi, M. E. Berend, M. A. Ritter, and R. M. Nunley, "Why Are Total Knees Failing Today? Etiology of Total Knee Revision in 2010 and 2011," *J. Arthroplasty*, vol. 28, no. 8, pp. 116–119, 2013.
- [10] Y. Achermann, M. Vogt, M. Leunig, J. Wüst, and A. Trampuz, "Improved diagnosis of periprosthetic joint infection by multiplex PCR of sonication fluid from removed implants," J. Clin. Microbiol., vol. 48, no. 4, pp. 1208–1214, 2010.
- [11] P. C. Matthews, A. R. Berendt, M. A. McNally, and I. Byren, "Diagnosis and management of prosthetic joint infection," *BMJ*, vol. 338, 2009.

- [12] A. Gaudin, G. Amador del Valle, A. Hamel, V. Le Mabecque, A.-F. Miegeville, G. Potel, J. Caillon, and C. Jacqueline, "A new experimental model of acute osteomyelitis due to methicillin-resistant Staphylococcus aureus in rabbit," *Lett. Appl. Microbiol.*, vol. 52, no. 3, pp. 253–257, 2011.
- [13] E. Moran, I. Byren, and B. L. Atkins, "The diagnosis and management of prosthetic joint infections," J. Antimicrob. Chemother., vol. 65, no. suppl 3, pp. iii45–iii54, 2010.
- [14] A. G. D. Valle, M. Bostrom, B. Brause, C. Harney, and E. A. Salvati, "Effective bactericidal activity of tobramycin and vancomycin eluted from acrylic bone cement," *Acta Orthop.*, vol. 72, no. 3, pp. 237–240, 2001.
- [15] T. Miclau, L. E. Dahners, and R. W. Lindsey, "In vitro pharmacokinetics of antibiotic release from locally implantable materials," J. Orthop. Res., vol. 11, no. 5, pp. 627–632, 1993.
- [16] P. V. Giannoudis, H. Dinopoulos, and E. Tsiridis, "Bone substitutes: an update," *Injury*, vol. 36, no. 3, pp. S20–S27, 2005.
- [17] B. M. DESAI, "Osteobiologics," Am. J. Orthop., vol. 36, no. 4S, pp. 8-11, 2007.
- [18] S. Radin, J. T. Campbell, P. Ducheyne, and J. M. Cuckler, "Calcium phosphate ceramic coatings as carriers of vancomycin," *Biomaterials*, vol. 18, no. 11, pp. 777–782, 1997.
- [19] J. A. Roberts, P. Kruger, D. L. Paterson, and J. Lipman, "Antibiotic resistance--what's dosing got to do with it?," *Crit. Care Med.*, vol. 36, no. 8, pp. 2433–2440, Aug. 2008.
- [20] M. P. Bostrom and D. A. Seigerman, "The clinical use of allografts, demineralized bone matrices, synthetic bone graft substitutes and osteoinductive growth factors: a survey study," HSS J., vol. 1, no. 1, pp. 9–18, 2005.
- [21] H. Winkler, O. Janata, C. Berger, W. Wein, and A. Georgopoulos, "In vitro release of vancomycin and tobramycin from impregnated human and bovine bone grafts," *J. Antimicrob. Chemother.*, vol. 46, no. 3, pp. 423–428, 2000.
- [22] T. N. Peel, K. L. Buising, and P. F. Choong, "Diagnosis and management of prosthetic joint infection," Curr. Opin. Infect. Dis., vol. 25, no. 6, pp. 670–676, 2012.
- [23] A. E. Brooks, B. D. Brooks, S. N. Davidoff, P. C. Hogrebe, M. A. Fisher, and D. W. Grainger, "Polymer-controlled release of tobramycin from bone graft void filler," *Drug Deliv. Transl. Res.*, vol. 3, no. 6, pp. 518–530, Dec. 2013.
- [24] S. N. Davidoff, J. O. Sevy, B. D. Brooks, D. W. Grainger, and A. E. Brooks, "Evaluating antibiotic release profiles as a function of polymer coating formulation-biomed 2011.," *Biomed. Sci. Instrum.*, vol. 47, p. 46, 2011.
- [25] D. R. Osmon, E. F. Berbari, A. R. Berendt, D. Lew, W. Zimmerli, J. M. Steckelberg, N. Rao, A. Hanssen, and W. R. Wilson, "Diagnosis and management of prosthetic joint infection: clinical practice guidelines by the Infectious Diseases Society of America," *Clin. Infect. Dis.*, vol. 56, no. 1, pp. e1–e25, 2013.
- [26] D. Neut, H. van de Belt, J. R. van Horn, H. C. van der Mei, and H. J. Busscher, "The effect of mixing on gentamicin release from polymethylmethacrylate bone cements," Acta Orthop. Scand., vol. 74, no. 6, pp. 670–676, Dec. 2003.
- [27] B. D. Brooks, S. N. Davidoff, D. W. Grainger, and A. E. Brooks, "Comparisons of Release of Several Antibiotics from Antimicrobial Polymer-Coated Allograft Bone Void Filler," *Open Antimicrob. Agents J.*, vol. In Press.
- [28] B. Mousset, M. A. Benoit, C. Delloye, R. Bouillet, and J. Gillard, "Biodegradable implants for potential use in bone infection," *Int. Orthop.*, vol. 19, no. 3, pp. 157–161, Jun. 1995.
- [29] E. J. Begg and M. L. Barclay, "Aminoglycosides--50 years on.," Br. J. Clin. Pharmacol., vol. 39, no. 6, pp. 597–603, Jun. 1995.
- [30] M. Brandl and L. Gu, "Degradation of tobramycin in aqueous solution," *Drug Dev. Ind. Pharm.*, vol. 18, no. 13, pp. 1423–1436, Jan. 1992.
- [31] C. Walsh, "Molecular mechanisms that confer antibacterial drug resistance," *Nature*, vol. 406, no. 6797, pp. 775–781, 2000.
- [32] B. D. Brooks, A. E. Brooks, and D. W. Grainger, "Antimicrobial Medical Devices in Preclinical Development and Clinical Use," in *Biomaterials Associated Infection*, T. F. Moriarty, S. A. J. Zaat, and H. J. Busscher, Eds. Springer New York, 2013, pp. 307–354.
- [33] F. Suarez, A. Monje, P. Galindo-Moreno, and H.-L. Wang, "Implant Surface Detoxification: A Comprehensive Review," *Implant Dent.*, vol. 22, no. 5, pp. 465–473, 2013.
- [34] Brooks, B.D., Sinclair, K., Davidoof, S.N., Williams, A., Lawson, S, Coates, B., Grainger, D.W., and Brooks, A.E., "Molded Polymer-Coated Composite Bone Void Filler Improves Tobramycin Controlled Release Kinetics," J. Biomed. Mater. Res. Part B - Appl. Biomater., In Press.
- [35] CLSI, "Performance Standards for Antimicrobial Susceptibility Testing; Seventeenth Informational Supplement," Clinical Laboratory Standards Institute, Jan. 2007.
- [36] W. K. Jung, H. C. Koo, K. W. Kim, S. Shin, S. H. Kim, and Y. H. Park, "Antibacterial activity and mechanism of action of the silver ion in Staphylococcus aureus and Escherichia coli," *Appl. Environ. Microbiol.*, vol. 74, no. 7, pp. 2171–2178, 2008.

- [37] J. R. Anderson, D. T. Chiu, R. J. Jackman, O. Cherniavskaya, J. C. McDonald, H. Wu, S. H. Whitesides, and G. M. Whitesides, "Fabrication of topologically complex three-dimensional microfluidic systems in PDMS by rapid prototyping," *Anal. Chem.*, vol. 72, no. 14, pp. 3158–3164, 2000.
- [38] H. van de Belt, D. Neut, W. Schenk, J. R. van Horn, H. C. van der Mei, and H. J. Busscher, "Gentamicin release from polymethylmethacrylate bone cements and Staphylococcus aureus biofilm formation," *Acta Orthop. Scand.*, vol. 71, no. 6, pp. 625–629, Dec. 2000.
- [39] C. Horner, D. Mawer, and M. Wilcox, "Reduced susceptibility to chlorhexidine in staphylococci: is it increasing and does it matter?," *J. Antimicrob. Chemother.*, p. dks284, Jul. 2012.